## **Supporting Information**

# High-Throughput Synthesis of Single-Layer MoS<sub>2</sub> Nanosheets as a Near-Infrared Photothermal-Triggered Drug Delivery for Effective Cancer Therapy

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#### 1. Supporting Discussion

# Calculation of the photothermal conversion efficiency

The photothermal conversion efficiency ( $\mu$ ) of MoS<sub>2</sub>-CS was determined according to the reported method by Lu *et al.* and Hu *et al.*<sup>1,2</sup> The detailed calculation was given as following:

During the photothermal heating process, the total energy balance can be expressed as

$$\sum_{i} m_{i} C_{p,i} \frac{dT}{dr} = Q_{laser} - Q_{Surr} \tag{1}$$

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where, m (g) and  $C_p(J/(g^{\circ}C))$  are the mass and constant-pressure heat capacity of water, respectively, T (°C) is the solution temperature at time t,  $Q_{laser}$  (mW) is the energy arising from the laser irradiation, and  $Q_{Surr}$  (mW) is the energy dissipated from the system surface to the surrounding environment.

For  $Q_{laser}$ , there are two contributions. One is the energy inputted by  $MoS_2$ -CS in the dispersion,  $Q_{NS}$ , as given by equation (2),

$$Q_{NS} = I(1 - 10^{-A_1})\eta \tag{2}$$

where I (mW/cm<sup>2</sup>, 1000 mW/cm<sup>2</sup>) is the laser power,  $A_{\lambda}$  is the absorbance of MoS<sub>2</sub>-CS at the wavelength of 808 nm (Figure S7b), and  $\eta$  is the conversion efficiency from the absorbed light energy to thermal energy.

The other is the absorbance by the cuvette walls and the solution,  $Q_{Dis}$  (mW). It is measured independently to be 29.89 mW using pure water without MoS<sub>2</sub>-CS. So, we obtain

$$Q_{laser} = Q_{NS} + Q_{Dis} = I(1 - 10^{-A_A})\eta + 29.89$$
 (3)

In addition, the energy dissipation is usually expanded as Taylor series of  $\Delta T$ . In our experiment, the first term is employed, which gives

$$Q_{Surr} = hS\Delta T = hS(T - T_{Surr})$$
(4)

Where h (mW/(m<sup>2</sup>•°C)) is heat transfer coefficient, S (m<sup>2</sup>) is the surface area of the container, and  $T_{Surr}$  is ambient temperature of the surroundings.

When the heat input is equal to heat output, the system reaches the steady state, and the temperature rises to a maximum,  $T_{\text{Max}}(^{\circ}\text{C})$ . In this case, the left side of Equation (6) becomes zero, we then obtain

$$Q_{laser} = Q_{Surr} \tag{5}$$

Combining Equation (2-5),  $\eta$  is therefore given by

$$\eta = \frac{hS(T_{Max} - T_{SUYY}) - Q_{Bis}}{I(1 - 10^{-A_{SDS}})} \tag{6}$$

To get the hS, we herein introduce  $\theta$  using the maximum system temperature,  $T_{max}$ 

$$\theta = \frac{T - T_{Surr}}{T_{Max} - T_{Surr}} \tag{7}$$

and a sample system time constant  $\tau_s(s)$ 

$$\tau_{s} = \frac{\sum_{i} m_{i} c_{p,i}}{h s} \tag{8}$$

Substituting Equation (6-7) into Equation 1, we obtain

$$\frac{d\theta}{dt} = \frac{1}{\tau_s} \left[ \frac{Q_{NS} + Q_{Dis}}{hS(T_{Max} - T_{Sarr})} - \theta \right]$$
(9)

At the cooling stage of the aqueous dispersion of  $MoS_2$ -CS, the laser was shut off, the  $Q_{NS}+Q_{Dis}=0$ . In this case, Equation (9) becomes

$$dt = -\tau_s \frac{d\theta}{\theta} \tag{10}$$

Integrating Equation (10), we obtain

$$t = -\tau_s \ln \theta \tag{11}$$

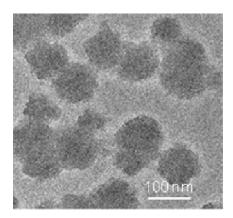
Therefore, time constant is determined to be  $\tau_s$ =202.75 s by applying the linear time data from the cooling period (after 600 s) vs-Ln $\theta$  (Figure 3c,d). Afterwards, according to Equation (11), the hS is deduced to be 10.36 mW/°C. Substituting 10.36 mW/°C into Equation (5), the 808 nm laser heat conversion efficiency ( $\eta$ ) of MoS<sub>2</sub>-CS can be calculated to be 24.37%.

### References

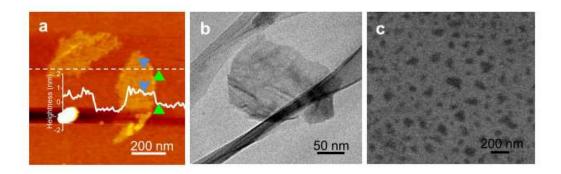
[1] Tian, Q.; Jiang, F.; Zou, R.; Liu, Q.; Chen, Z.; Zhu, M.; Yang, S.; Wang, J.; Wang, J.; Hu, J. Hydrophilic Cu<sub>9</sub>S<sub>5</sub> Nanocrystals: A Photothermal Agent with a 25.7% Heat Conversion Efficiency for Photothermal Ablation of Cancer Cells *in Vivo. ACS Nano* **2011**, *5*, 9761-9771.

[2] Liu, Y.; Ai, K.; Liu, J.; Deng, M.; He, Y.; Lu, L. Dopamine-Melanin Colloidal Nanospheres: An Efficient Near-Infrared Photothermal Therapeutic Agent for *In Vivo* Cancer Therapy. *Adv. Mater.* **2013**, *25*, 1353-1359.

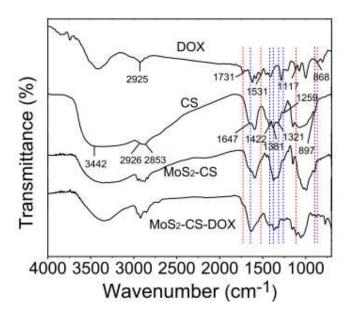
# 2. Supporting Figures



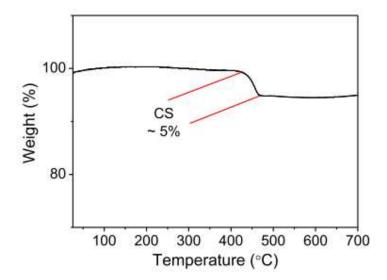
**Figure S1.** Typical TEM image of MoS<sub>2</sub>-CS nanosheets.



**Figure S2.** Typical (a) AFM, (b) TEM, and (c) SEM images of  $MoS_2$  nanosheets prepared *via* sonication for 1 h. This result showed that  $MoS_2$ -based nanosheets could be obtained by changing the sonication time.



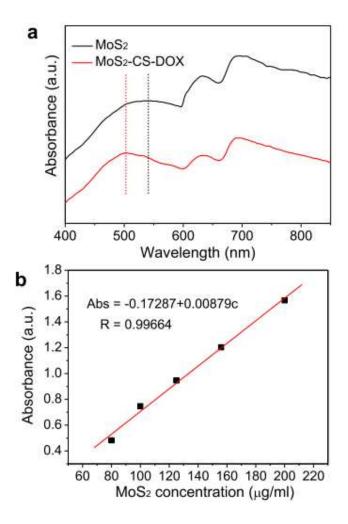
**Figure S3** FT-IR spectra of DOX, CS, MoS<sub>2</sub>-CS and MoS<sub>2</sub>-CS-DOX, respectively. For MoS<sub>2</sub>-CS, the peak appearing at 3442 cm<sup>-1</sup> was due to the stretching vibration of N-H bond. Both the -CH<sub>2</sub>- strength vibration (2840-2960 cm<sup>-1</sup>) and the internal vibration of the amide bonds (1320-1650 cm<sup>-1</sup>) of CS molecules were also observed in the FT-IR of MoS<sub>2</sub>-CS. These results indicated that CS molecules were successfully attached onto the surface of MoS<sub>2</sub> nanosheets. After DOX molecules were further adsorbed on the MoS<sub>2</sub>-CS nanosheets, the additional absorption band were observed at 1731 cm<sup>-1</sup>, which was attributed to the carbonyl peaks of DOX. The peak centered at 868 cm<sup>-1</sup>corresponded to primary amine -NH<sub>2</sub> wag vibration from DOX. These observations further confirmed the successful loading of DOX to MoS<sub>2</sub>-CS. The obtained results were also in good agreement with an earlier report.



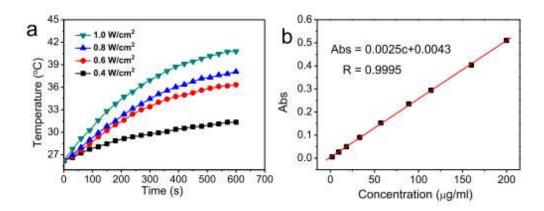
**Figure S4.** Thermal gravimetric (TGA) analysis of the  $MoS_2$ -CS nanosheets. The weight-loss region (400-450 °C) should be attributed to the decomposition of CS molecules. The amount of CS molecules was determined to be ca. 5 wt%, indicating that CS molecules were really adsorbed on the surface of  $MoS_2$ -CS.



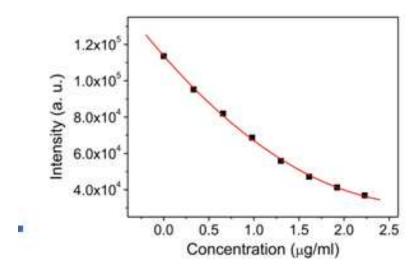
**Figure S5.** A large amount of with whole volume of 100 ml of MoS<sub>2</sub>-CS dispersed in deionized water for more than 20 days. The concentration is  $\sim$ 1.0 mg/ml.



**Figure S6.** (a) UV-vis absorbance spectra of  $MoS_2$ -CS and  $MoS_2$ -CS-DOX. DOX loaded on  $MoS_2$ -CS was evidenced by an additional absorption peak centered at ~500 nm. (b) Plots of linear fitting extinction *versus* wavelength for  $MoS_2$ -CS aqueous solution with various concentrations at 691 nm, which was used to determine the concentration of the unknown  $MoS_2$ -CS aqueous dispersions.



**Figure S7.** (a) The temperature elevation of MoS<sub>2</sub>-CS aqueous solution (100 μg/ml) irradiated by 808-nm laser with different power density *versus* a function of irradiation time (0-10 min). These results suggested that the temperature gradually increased with the increase of power densities, showing a power-dependent manner. (b) Plots of linear fitting extinction *versus* wavelength for MoS<sub>2</sub>-CS in aqueous solution with various concentrations at absorption peak of 808 nm.



**Figure S8.** A quenching of the fluorescence when the DOX is linked at the  $MoS_2$ -CS with respect to the free DOX.

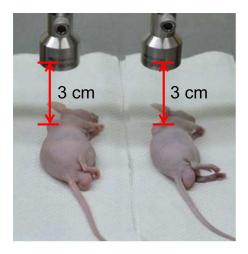
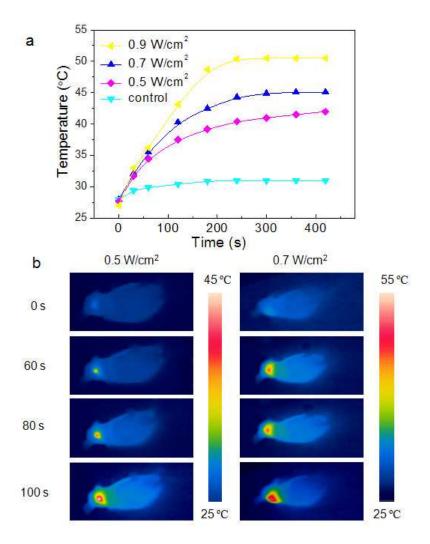
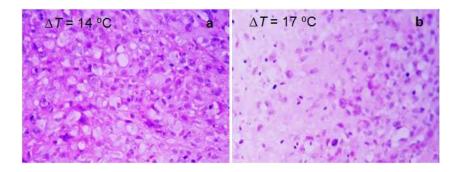


Figure S9. Photothermal therapy setup showing laser and the Panc-1-bearing mice.



**Figure S10.** (a) The temperature changes on tumors of mice under different treatments. (b)Infrared thermal images of Panc-1 tumor-bearing mice injected with MoS<sub>2</sub>-CS-DOXwhich were exposed to an 808 nm laser at different output power densities.



**Figure S11.** Histological images of tumors collected from the groups of MoS<sub>2</sub>-CS-DOX+NIR 808-nm laser with different power densities.